

#### **INVIVE-Approx**

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Summary

# Simulating the human respiratory system from an approximation perspective

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# Ventilator induced diaphragmatic dysfunction





- Mechanical ventilation of intensive care patients leads to *Ventilator induced diaphragmatic dysfunction* (VIDD).
- In normal breathing the diaphragm contracts, but ventilation stretches the muscle.
- Significant loss off function in short time,  $\mathcal{O}(24h)$ .
- Goal: Understand effect, reduce effect, plan rehabilitation.

E. Larsson, Nov 30, 2021 (2:23)



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# The INVIVE project



Application: Biomechanical modeling of the respiratory system to evaluate and improve mechanical ventilation.





- Raw geometry data—3D medical images.
- Segmented data—Noisy and locally biased.
- Pressure, volume and geometry time series data.

### Desired outcomes:

- Smooth geometry reconstruction.
- Simulation of muscle tissue during ventilation.

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# Radial basis function (RBF) approximation

Scaled translates  $\varphi(\varepsilon ||\underline{x} - \underline{x}_j||)$  of positive definite function  $\varphi(r)$  such as the Gaussian.

### Approximations

$$\widetilde{\mu}(\underline{x}) = \sum_{j=1}^{N} \lambda_j \phi(\varepsilon \| \underline{x} - \underline{x}_j \|)$$

Differentiation

$$\mathcal{L}\tilde{u}(y) = \sum_{j=1}^{N} \lambda_j \mathcal{L}\phi(\varepsilon \| \underline{y} - \underline{x}_j \|)$$

### Advantages

- Meshfree flexible with respect to geometry.
- Spectrally accurate approximations.
- Ease of implementation.

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# Geometry design objectives and approach

### The surface representation



- Implicit surface given by zero level set.
- Localized approximations to keep cost low.
- Infinitely smooth representation (globally).
- ► No spurious zero level sets.



### Approach to reach target

- Decouple basis location from data.
- Anisotropic local approximations.
- Extra stabilizing conditions.



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### Partition of unity method for thin structures

- Global approximation  $\tilde{u}(\underline{x}) = \sum_{j=1}^{P} w_j(\underline{x}) \tilde{u}_j(\underline{x})$  P – the number of patches
  - $w_j$  partition of unity weight function
  - $\tilde{u}_j$  patch local radial basis function approximation
- One layer of cylindrical patches.
- The patches are adapted to the geometry.







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### The adaptive cover generation



- Initial clustering of points using kmeans.
- Cylindrical patches are fitted to the data using PCA.
- Thick patches (large curvature) are subdivided.
- Finally an overlap  $\delta$  is enforced between patches.



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## Partition of unity weight functions

Cylindrical reference patch with radius R and height H.

Choose a basic function  $\begin{cases} \psi_0(r) > , 0 & 0 \le r < 1, \\ \psi_0(r) = 0, & r \ge 1. \end{cases}$ 

Local generating function  $\psi(\underline{x}') = \psi_0\left(\frac{r'}{R}\right)\psi_0\left(\frac{x'_d}{H/2}\right)$  positive on the patch and zero on the patch boundary.

Normalize with Shepard's method  $w_j(\underline{x}) = \frac{\psi_j(\underline{x})}{\sum_{i=1}^{P} \psi_i(\underline{x})}$ .



Overlap determines gradients. Non-smooth at outer boundary intersections.

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## The local geometry approximations

RBF approximation of local level set function



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(Some points outside are included.)

- Unit component in normal direction.
- Additional distance values.

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### Smooth geometry reconstruction

Infinitely smooth weight functions (from bump function) and RBFs (multiquadrics) are used.

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# Solving a PDE in the diaphragm geometry

Challenges

- Complex, thin, non-parametric geometry.
   Representation, resolution, node generation.
- Pressure conditions on large parts of the boundary.

Conditioning/sensitivity to node layout.

### Solution approaches

- Oversampled RBF methods for stability. RBF-PUM: Larsson, Shcherbakov Heryudono 2017. RBF-FD: Tominec, Larsson, Heryudono 2021.
- Unfitted RBF methods for nodes and resolution. *Tominec, Breznik 2021.*

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# **Oversampled RBF-FD**

For a point  $\underline{x}_c$  pick  $n \ll N$  neighbours  $\underline{x}_j$ ,  $j = 1, \ldots, n$ We interpolate  $u(\underline{x}_i)$  using  $\phi(r) = r^3$  and monomials  $p_i$ 

$$\tilde{u}(\underline{x}) = \sum_{j=1}^{n} \lambda_j \phi(\|\underline{x} - \underline{x}_j\|_2) + \sum_{j=1}^{m} \mu_j p_j(\underline{x})$$

under the constraint 
$$\sum_{j=1}^{n} \lambda_j p_k(\underline{x}_j) = 0, \ k = 1, \dots, m.$$
  
We enforce the PDE and boundary conditions at points

in the Voronoi region around  $x_c$ 

$$\mathcal{L}\tilde{u}(\underline{y}) = \sum_{j=1}^{n} \lambda_j \mathcal{L}\phi(\|\underline{y} - \underline{x}_j\|_2) + \sum_{j=1}^{m} \mu_j \mathcal{L}p_j(\underline{y}).$$

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Continuous least-squares approximation for Poisson with mixed boundary conditions

Continuous norm and homogeneous space  $L_2$ -norm  $||u||_{\Omega}^2 = (u, u)_{L_2(\Omega)} = \int_{\Omega} |u(y)|^2 dy$ .  $V^0 = \{v \in W_2^2(\Omega) : v|_{\partial\Omega_D} = 0\}.$ 

Least-squares for the PDE problem Minimize  $\|\Delta u - f\|_{\Omega}^2 + \|\frac{\partial u}{\partial n} - g\|_{\partial\Omega_N}^2 + \|u - h\|_{\partial\Omega_D}^2$ . Write as:  $u \in V$  such that  $a(u, v) = \ell(f, v)$ ,  $\forall v \in V$ , where  $a(u, v) = (\Delta u, \Delta v)_{\Omega} + (\frac{\partial u}{\partial n}, \frac{\partial v}{\partial n})_{\partial\Omega_N} + (u, v)_{\partial\Omega_D}$ .

### Coercivity of the bilinear form

$$C^2a(v,v) \geq \|v\|_{\Omega}^2, \quad v \in V^0.$$

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### Discrete $\leftrightarrow$ semi-discrete

Let  $v_h$  be the discontinuous RBF-FD-LS approximation and define a fully discrete norm from  $(f,g)_{\ell_2(\Omega)} = \frac{|\Omega|}{M} \sum_{i=1}^M f(y_i)g(y_i).$ 

This is a discretization of the semi-discrete inner product  $(f,g)_{L^*(\Omega)} = \sum_{k=1}^N (f,g)_{L_2(\mathcal{V}_k)}$  ( $\mathcal{V}_k$  Voronoi regions),



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### Semi-discrete $\leftrightarrow$ continuous

Let  $\mathbf{v} = S(\mathbf{v}_h) \in W_2^2(\Omega)$  be the smoothed counterpart of  $\mathbf{v}_h$ We can show that



 $\eta_0$  and  $\eta_a$  in practice become smaller with smoother data, but do not depend on the oversampling M. 

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### Stability estimate: Coercivity

$$\begin{aligned} \|v_{h}\|_{\ell_{2}(\Omega)}^{2} &\leq (1+\tau)\|v_{h}\|_{L_{2}^{*}(\Omega)}^{2} \\ &\leq (1+\tau)(1+\eta_{0})\|v\|_{L_{2}(\Omega)}^{2} \\ &\leq (1+\tau)(1+\eta_{0})C^{2}a(v,v) \\ &\leq (1+\tau)(1+\eta_{0})C^{2}(1+\eta_{a})a^{*}(v_{h},v_{h}) \\ &\leq \frac{(1+\tau)(1+\eta_{0})C^{2}(1+\eta_{a})}{1-\tau}a_{h}(v_{h},v_{h}). \end{aligned}$$

 $\tau$ —quadrature error, decreases with # equations M.  $\eta_0$ ,  $\eta_a$ —smoothing errors, decrease with smoothness. C—coercivity bound for functions in  $W_2^2(\Omega)$ , fixed.

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# Convergence: Consistency

- ▶ Polynomial basis of degree *K*,  $m = \frac{(K+1)\cdots(K+d)}{d!}$ .
- Stencil size  $n \ge 2m$ , larger if skewed.
- Well-distributed, but preferably not Cartesian nodes.

### Theorem Bayona 2019

Then  $|\mathcal{L}u(\underline{x}) - \sum_{j=1}^{n} \mathcal{L}\psi_j(\underline{x})| = \mathcal{O}(h^{K+1-\alpha})$ , where  $\alpha$  is the order of the operator  $\mathcal{L}$ , and h measures node distance.



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### The final convergence estimate

For a Poisson problem with Dirichlet and Neumann boundary conditions, and polynomials of degree K

$$e\|_{\ell_{2}(\Omega)} \leq \sqrt{2}C\left(\frac{(1+\tau)(1+\eta_{0})(1+\eta_{a})}{1-\tau}\right)^{\frac{1}{2}} \\ (c_{1}h^{K+1}+c_{2}h^{K}+c_{2}h^{K-1})|u|_{W_{\infty}^{K+1}(\Omega)}.$$

- ► Convergence rate determined by the degree *K*.
  - Optimal convergence requires sufficient smoothness.

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• Error decreases mainly with h, but also with  $M^{-1}$ .

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### Run-time comparison



- Least-squares RBF-FD is more efficient.
- Efficiency almost independent of M = qN.
- High accuracy, more benefit from large K.

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### Linear elasticity in cross section



- Model problem: Linear elasticity with manufactured Dirichlet and traction conditions.
- Method: Oversampled RBF-FD

Tominec, Larsson, Heryudono 2021

Smoothed boundary conditions

arXiv preprint: Tominec, Villard, Larsson, Bayona, Cacciani 2021

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# Unfitted RBF-FD on the whole diaphragm

A Poisson problem with mixed boundary conditions is solved in the diaphragm geometry.

Unfitted nodes Error distribution Largest error here  $\approx 5 \cdot 10^{-3}$ 

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Using localized oversampled RBF methods, we can

- reconstruct non-trivial smooth geometries in a controlled way, and
- solve PDE model problems in these geometries at a reasonable cost.

To model a real diaphragm, we further need

- a proper tissue model, including active muscle contraction, and
- real boundary conditions given by the abdominal pressure, the thoracic pressure, and the attachment to the ribs and spine.

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